# Role of protonation states in stability of molecular dynamics simulations of high-resolution membrane protein structures

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#### 23 Abstract

24 Classical molecular dynamics (MD) simulations provide unmatched spatial and time 25 resolution of protein structure and function. However, accuracy of MD simulations often 26 depends on the quality of force field parameters and the time scale of sampling. Another 27 limitation of conventional MD simulations is that the protonation states of titratable amino 28 acid residues remain fixed during simulations, even though protonation state changes 29 coupled to conformational dynamics are central to protein function. Due to the uncertainty 30 in selecting protonation states, classical MD simulations are sometimes performed with all 31 amino acids modeled in their standard charged states at pH 7. Here we performed and 32 analyzed classical MD simulations on high-resolution cryo-EM structures of two membrane 33 proteins that transfer protons by catalyzing protonation/deprotonation reactions. In 34 simulations performed with amino acids modeled in their standard protonation state the 35 structure diverges far from its starting conformation. In comparison, MD simulations 36 performed with pre-determined protonation states of amino acid residues reproduce the 37 structural conformation, protein hydration, and protein-water and protein-protein interactions of the structure much better. The results suggest it is crucial to perform basic 38 39 protonation state calculations, especially on structures where protonation changes play an 40 important functional role, prior to launching any MD simulations. Furthermore, the combined 41 approach of protonation state prediction and MD simulations can provide valuable 42 information on the charge states of amino acids in the cryo-EM sample. Even though accurate 43 prediction of protonation states currently remains a challenge, we introduce an approach of 44 combining pKa prediction with cryo-EM density map analysis that helps in improving not only 45 the protonation state predictions, but also the atomic modeling of density data. 46

47 Keywords; molecular dynamics, protonation states, pKa calculations, cryo-electron48 microscopy, electrostatics.

## 49 Introduction

50 Within the past decade, the resolution of single-particle cryo-EM structures has improved 51 dramatically, largely due to the improvements in direct electron detectors and processing software <sup>1</sup>. The resolution of single-particle cryo-EM structures is now comparable to x-ray 52 crystallography and NMR structures, and the so-called "resolution revolution" has made it 53 54 possible to determine structures of many previously inaccessible complexes, particularly for 55 membrane proteins<sup>2</sup>. Many of these structures have a resolution below 2.5 Å, allowing 56 accurate modeling of protein conformations, including ordered water molecules, which has 57 significant implications in drug design<sup>3</sup> and is also central to our understanding of the molecular mechanism of enzymes that catalyze proton transfer reactions<sup>4</sup>. 58

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Proton transfer can take place across a chain of water molecules via a Grotthuss-type 60 mechanism <sup>5</sup>. However, proton transfer routes through proteins do not consist only of water 61 62 molecules but are often made up of hydrogen-bonded networks of polar and charged amino 63 acid residues. Besides titratable residues such as glutamic acid and lysine, which can donate 64 or accept protons, other residues that are part of these networks include asparagine and 65 glutamine, and serine, threonine, and tyrosine with hydroxyl groups in their sidechains. These 66 polar residues can not only assist in proton transfer reactions by stabilizing charged 67 intermediates but may also undergo protonation/deprotonation reactions in proteinaceous environments<sup>4, 6-8</sup>. Moreover, titratable acidic and basic residues are well-known to act as 68 proton transfer elements and proton loading sites in several enzymes <sup>4, 9, 10</sup>. However, the 69 70 protonation states in protein structures are usually not explicitly modelled. Such information 71 can be obtained with neutron diffraction techniques, but only for relatively small proteins <sup>11</sup>.

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73 The two main structure determination methods for protein complexes, x-ray crystallography 74 and cryo-EM, produce superficially similar results. However, they differ fundamentally in the 75 way atomic structures are imaged. X-rays are deflected by electrons and thus produce 76 electron density maps, but electrons are scattered by Coulomb potential, and they are thus 77 sensitive to charges. While positively charged ions just add extra density to an already positive 78 signal, negative charges, in particular O<sup>-</sup>, can give rise to negative electron scattering amplitudes <sup>12-14</sup>. As a result, negatively charged sidechains of glutamate and aspartate 79 80 residues are not visible in cryo-EM maps. Although the weak density of these sidechains has sometimes been interpreted as a result of the radiation sensitivity of the carboxyl group <sup>15, 16</sup>, 81 the former mechanism appears to have a larger contribution <sup>14, 17-19</sup>. The absence of sidechain 82 83 density hampers accurate model building. On the other hand, it makes it possible to 84 determine the charge state of acidic residues.

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To complement cryo-EM structures, molecular dynamics (MD) simulations are often 86 87 performed <sup>20-30</sup>. These help in studying the dynamics of the protein and the solvent, as well 88 as the binding and unbinding of lipids, ligands, and ions. The approach of combining structural 89 data with MD simulations is a powerful technique to understand protein structure and 90 function. The abundance of new structures gives plenty of opportunity to perform these 91 simulations routinely at various levels of computational approximations. However, one limitation of conventional molecular dynamics is that covalent bonds are fixed throughout 92 93 the simulation, therefore the charge states of titratable residues (often selected as the 94 standard charge state that is Asp/Glu deprotonated, Lys/Arg protonated and His neutral) 95 remain unchanged. This results in a biased scenario, and biologically relevant conformational

96 states with alternative protonation states are not populated. Moreover, situations where 97 changes in protonation states can occur as a function of conformational dynamics (e.g. 98 membrane proteins catalyzing proton transfer) are also not captured. However, there are 99 various methods that can allow charge states of amino acids to change during MD 100 simulations, such as hybrid QM/MM MD, and constant pH MD, but these are generally 101 computationally costly <sup>31</sup>, although there have been recent improvements in the enhanced 102 scalability of constant pH MD <sup>32</sup>.

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For many proteins, performing MD simulations by systematic altering of charge states of individual titratable residues is unrealistic, due to the large number of such residues. Of course, one can alter protonation states of selected conserved residues to study specific questions, and this has indeed been performed to obtain valuable functional insights <sup>33-37</sup>. However, due to the long-range nature of electrostatic interactions the protonation state of one titratable residue affects another's by ca. 8 kcal/mol (with a separation of 10 Å at  $\epsilon$ =4) and such aspects are often ignored when performing simulations.

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112 Alternatively, one can calculate the pKa of all titratable residues in a protein for a given conformational state (obtained from a cryo-EM experiment, for example) and perform MD 113 114 simulations in that fixed protonation state. There are several methods to perform pKa 115 calculations, many of which are based on continuum electrostatics approaches <sup>38</sup>. However, these require a significant amount of preprocessing and can display large variation in pKa 116 117 values due to subtle conformational changes. Alternatively, empirical methods, such as Propka can be employed relatively easily, to give fast and sufficiently accurate predictions of 118 the pKa of all ionizable groups present in a protein, even if hundreds in number <sup>39</sup>. Methods 119 120 like Propka <sup>40</sup>, often give reasonable estimates for the pKa of buried titratable residues, in 121 particular if the sites are far from any redox active cofactors. Due to their rapid pKa 122 estimations, they can be used on thousands of simulation snapshots to obtain profiles of pKa 123 change as a function of conformational dynamics <sup>35, 41</sup>. Similarly, Monte Carlo-based pKa prediction methods have also been used to predict charged states of systems, either using 124 standalone PDB files or simulation snapshots <sup>42</sup>. 125

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127 In this study, we present MD simulations on two high-resolution cryo-EM structures of 128 membrane proteins. The two structures are the respiratory complex I from Yarrowia lipolytica (PDB 7071, EMD-12742) <sup>43</sup> and the multiple resistance and pH adaptation (Mrp) 129 130 cation/proton antiporter from *Bacillus pseudofirmus* (PDB 7QRU, EMD-14124) <sup>44</sup>. Both 131 proteins facilitate proton transfer reactions that involve amino acid residues and water 132 molecules, many of which have been resolved in the two structures. The role of protein 133 hydration, water dynamics as well as change in protonation state is central to the structure 134 and function of these proteins. By performing long time scale MD simulations in multiple 135 charge states of these proteins and extensively analyzing protein and solvent dynamics, we show that both proteins deviate from the original cryo-EM conformation when simulated in 136 137 the standard protonation state of titratable amino acid residues, while MD simulations in pre-138 defined protonation states stabilize the protein conformation much better. We propose that the approach of protonation state prediction combined with MD simulations can give insights 139 140 into the charge state of residues in a cryo-EM structure. Furthermore, we find that the 141 prediction of protonation states of acidic residues agrees well with the charge state

assignment based on cryo-EM density maps, and that outliers can be identified with theapproach discussed here, leading to an improved modeling of cryo-EM density data.

#### Results 144

Two high-resolution membrane protein structures were chosen for this investigation. First, 145 146 the 2.1 Å resolution structure of complex I from Y. *lipolytica*, which is over 1 MDa in size, and has more than 1600 structural water molecules resolved <sup>43</sup>. Around 100 of these are in the 147 potential proton transfer pathways present in its membrane-bound subunits (Fig. 1). Second, 148 149 a structure from the evolutionarily related Na<sup>+</sup>/H<sup>+</sup> Mrp antiporter <sup>44</sup> at a similar resolution of 150 2.2 Å. This protein is much smaller than complex I (ca. 213 kDa) and consists of membrane-151 bound subunits only, without redox active cofactors. There are 360 water molecules resolved in the structure of the Mrp antiporter, around 70 of them in the potential proton and sodium 152 153 transfer pathways (Fig. 1). The structure of complex I contains more than 1300 titratable 154 residues, while the Mrp structure has around 200. We performed MD simulations on both complexes with all titratable sites either modeled in their standard states (S state) or based 155 156 on pKa calculations at pH 7 (P7 state). We find that in the P7 state, complex I has 68 157 neutralized titratable amino acids, out of which 25 are in the membrane core of the enzyme (Fig. 1), while in the Mrp antiporter 13 residues are neutralized in the P7 state. Accordingly, 158 159 the charge reduces from +90/-94 to +83/-76 in the complex I membrane arm, and from +116/-160 118 to +110/-112 in the Mrp upon neutralization of titratable sites as part of pKa calculations 161 (see Tables S1 and S2 for lists of residues neutralized in complex I and Mrp antiporter, 162 respectively). 163



MrpB MrpF

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165 Fig. 1 – Structure of the membrane domain of respiratory complex I (upper) and Mrp 166 antiporter (lower). The protein is shown in ribbon representation and colored by subunit. Only core membrane-bound subunits are shown in color for complex I, with the hydrophilic core 167 subunits shown as gray. Structurally resolved water molecules are shown as small green 168 spheres, with those in the functionally relevant hydrophilic axes of complex I and Mrp 169 170 antiporter shown as larger red spheres. Proton translocation is suggested to take place across 171 this axis, which is a vital part of the mechanism for both proteins. The inset in the upper panel shows a region of the complex I membrane arm within the high-resolution cryo-EM density 172 (grey mesh), including density for water molecules. 173

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#### 178 Global mobility of proteins in P7 and S states

179 First, the overall global mobility of both systems was analyzed in the S and P7 states. Fig. 2 180 shows the time series as well as the distribution of the RMSD (root mean square deviation) of 181 the backbone atoms for the core membrane-bound subunits of complex I and Mrp antiporter in the two simulation states. The P7 state systems with lower charge have overall lower RMSD 182 for both protein complexes, which means that the backbone atoms stay closer to the starting 183 conformation throughout the simulation. This notion is also true if a similar RMSD analysis is 184 185 performed on the C $\alpha$  backbone atoms and all protein atoms excluding hydrogens, even with 186 the inclusion of the hydrophilic domain of complex I (Fig. S1). 187





**Fig. 2** – RMSD (root mean square deviation) of the backbone atoms over time for both complex I (core membrane subunits, left panel) and Mrp antiporter (right panel) in S and P7 states. The upper plots show the RMSD as a time series, with each colored trace representing a different simulation replica. The thick lines show the moving average of 20 ns, while the thinner lines show the RMSD for every 1 ns. The bottom panels show the distribution of RMSD values in the S and P7 states using a kernel density estimate (KDE) function with combined data of all three replicas.

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Similarly, the RMSF (root mean square fluctuation), which measures the average amount an atom moves during the entire simulation, is also consistently found to be lower in the P7 states than in the S states. The boxplots in Fig. 3 show the RMSF of Cα atoms in each individual subunit of the Mrp antiporter. For all antiporter chains, lower RMSF values are observed in

202 the P7 state, indicating that there is an overall stability in the system as charges of titratable 203 sites are neutralized (based on pKa estimates). A similar trend was also observed in complex 204 I (Fig. S2). The spatial distribution of the RMSF data is shown in the lower panel of Fig. 3. MrpA 205 subunit (Figs. 1 and 3) has the largest number of titratable residues that undergo protonation 206 state changes to become neutralized and this has a clear impact in reducing the RMSF of the 207 subunit. Interestingly, the stability of the protein also increases in areas somewhat far from the residues that change protonation states (magenta spheres), highlighting that the charge 208 209 change of just a few titratable residues can have conformational changes imparted both at 210 the local and the global level.





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Fig. 3 – (Top) RMSF (root mean square fluctuation) of C $\alpha$  atoms in Mrp antiporter subunits, 212 calculated for all simulation data in S and P7 states. The box plots represent the distribution 213 214 of RMSF values for each subunit, in both states. The shaded box represents the interguartile 215 range, with the middle line showing the median. The upper and lower lines are the maximum 216 and minimum values respectively. (Bottom) The panel shows the protein structure colored 217 according to the extent of conformational change in the P7 state compared to the S state. Red represents  $C\alpha$  RMSF increased in the P7 state and blue represents a decrease. The 218 219 magenta spheres show the positions of residues that undergo a protonation state change in 220 P7 simulations.

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Overall, the key observation is that MD simulations performed in predefined protonation states retain a structure closer to the cryo-EM conformation for both protein complexes studied here. This in turn means that the simulated charge state is closer to the charge state

- of the protein during cryo-EM sample preparation. To understand why P7 state simulations show overall stability relative to the S state, we performed additional analyses.
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### 228 Water-protein interactions and protein hydration in P7 and S states

229 In the high-resolution structures of complex I and Mrp antiporter, the positions of several 230 water molecules are resolved. We therefore next analyzed how water-protein interactions 231 and protein hydration are affected in the S and P7 simulation states. The contacts between 232 all water molecules and protein were clearly reduced in the P7 states compared with the S 233 states (Fig. 3, upper panels). The lower charge in P7 states (+83/-76 compared to +90/-94 in S state of complex I and +110/-112 compared to +116/-118 in S state of Mrp antiporter) 234 235 prevents extensive hydration of the protein resulting in lower number of contacts between 236 water oxygens and protein. This is also reflected in the clear reduction of water contacts that 237 take place with the residues that change protonation state (Fig 3, middle panel).





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Fig. 3 – KDE plots for the number of water oxygen atoms in contact within 4 Å of protein residues, with the left column showing data for complex I (core membrane subunits) and the right for Mrp antiporter. Top panels show the number of waters in contact with all protein atoms, middle panels show for protein residues that change protonation state in P7 state simulations, and lower panels show the number of waters in contact with residues in the

functionally relevant horizontal axis (Fig. 1). Blue vertical lines in the lower panels indicate the number of waters resolved in the cryo-EM structures that are in contact with the residues in the central hydrophilic axis.

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In both proteins, a hydrophilic axis runs through the central part of the membrane domain, which is thought to be the structural basis for proton transfer reactions <sup>43-48</sup>. We next evaluated the time evolution of internal water molecules in this hydrophilic axis for both states in both proteins. We observed that the number of internal water molecules in the P7 state remains lower and closer to the water content observed in the structures, whereas in S state runs, extensive hydration of the proteins is observed (Fig. 3, lower panel and Fig. S3).

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256 Next, we analyzed the hydrogen bonding between the water molecules and the protein. The 257 time evolution of the hydrogen bonds between protein and structurally resolved water 258 molecules showed a more rapid decline in S states compared to the P7 states, with the latter 259 also displaying a slightly higher number of such interactions in long time scales (Fig. 4). This 260 indicates that although water exchange does take place in the P7 state, the exchange is less 261 rapid and a greater number of hydrogen bonds that existed in the initial structural state are maintained for long time scales. The stable water-protein hydrogen bonds combined with 262 263 lower hydration in the P7 state also suggests a lower water exchange rate in these simulations. The details of which protein-structural water hydrogen bonds are stabilized in 264 265 the Mrp antiporter is shown in Table S3, and notably the stabilization of these hydrogen bonds 266 is associated with a decrease in RMSF.

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In Mrp antiporter, in the S state most structural waters loose hydrogen bonds with the protein 268 269 residues in the µs time scale, whereas in P7 state the loss is relatively slower and less 270 extensive in the given time scales (Fig. 4). Interestingly, the loss of hydrogen bonds is much 271 more drastic in complex I simulations, especially in the shorter time scales. To further probe 272 into the kinetics of loss of hydrogen bonding between the structural waters and protein, we 273 fitted the profiles (Fig. 4, upper panels) to exponential function (see methods) and obtained 274 the half-life of protein-water hydrogen bonds  $(t_{1/2})$ . The results show that on average in 275 complex I P7 state hydrogen bonds survive longer (average  $t_{1/2} \sim 162$  ns) compared to S state 276 (average  $t_{1/2} \sim 113$  ns). For relatively shorter time scales (ca. 500 ns), a more subtle but similar 277 effect was also observed for Mrp antiporter simulations (average  $t_{1/2}$  ~135 ns in S state 278 compared to ~145 ns in P7 state).

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Fig 4 – Hydrogen bonds between protein and structural water molecules. (Top) The number
of hydrogen bonds throughout the S and P7 simulation trajectories are shown as a time series.
The different colors of traces represent different simulation replicas. (Bottom) The data from
all trajectories is shown in the lower panels as a density. Only the core membrane subunits of
complex I were considered for analysis. The hydrogen bonding distance was cut off at 3.5 Å
and the angle at 150<sup>°</sup>.

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#### 288 Protein-protein interactions

289 In addition to the protein-water hydrogen bonding interactions, protein-protein hydrogen 290 bonds were also analyzed. The number of protein-protein sidechain hydrogen bonds are 291 consistently found to be higher throughout the P7 state trajectories (Fig. 5). This implies that 292 structural stability is higher in P7 states compared to the S states for both Mrp antiporter and 293 complex I, as also observed in RMSD and RMSF analysis (see above). The lower number of 294 protein-protein interactions is also in agreement with the higher level of hydration observed 295 in the S state. In other words, enhanced water entry/exit in the protein causes protein-protein 296 interactions to be perturbed, resulting in structural destabilization. Specific pairs of residues 297 from the Mrp antiporter that showed a significant increase (>50 %) in hydrogen bonding are 298 shown in Table S4. Interestingly, although only two of the residue pairs undergo changes in 299 protonation state between S and P7 states, still several other pairs show enhancement in 300 hydrogen bonding occupancy, pointing out that long-range effects can occur upon charge 301 change.

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Fig. 5 – Number of hydrogen bonds between protein sidechains throughout the simulation
 for complex I and Mrp antiporter. Top panels show the time evolution of all hydrogen bonds
 for three different simulation replicas, with the hydrogen bonding distance cut off at 3.5 Å
 and the angle at 150°. Bottom panels show the same data as KDE plots. In case of complex I,
 only core subunits of the membrane arm are considered (see Fig. S4 for full protein).

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The above data on protein dynamics and hydration, as well as hydrogen bonding analysis in two different charge states lead to the conclusion that higher protein fluctuations are caused by extensive hydration, which in turn is caused by the highly charged state of the protein, as in the S state. The correct (or near-to-correct) charge state of the protein is thus critical for its structural stability. Hence, prior to launching long time scale MD simulations of highresolution membrane proteins, a proper charge analysis by means of pKa calculations is recommended.

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## 320 Simulations with different pH values

321 It is clear from the above analysis that the protein simulations that have charge states defined 322 by predetermined protonation states of titratable residues set at pH 7 are well-behaved and 323 are closer to the conformation obtained from cryo-EM. This is true for both global and local 324 mobility, as well as protein hydration. To further explore how altering protonation state 325 affects these characteristics, we performed a series of simulations of the Mrp antiporter 326 complex at 4 more pH values: 5, 6, 8, and 9. The RMSD of the protein (Fig. 6A) was lowest at 327 pH 6 and pH 7, with pH 5 showing the most instability. Similarly, both the number of water

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molecules in contact with protein (Fig. 6B) and the number of water molecules in the central
hydrophilic axis (Fig. 6C) was lowest for pH 6 and pH 7, with pH 5 deviating the most. At pH 5,
many of the negatively charged residues become neutral, and positive residues stay positive.
Importantly, many histidine residues become doubly protonated, which introduces excess
positive charge in several regions of the protein. As a result, bulk water molecules enter the
protein, causing instability in protein sidechains and loops, even more than in the S state.

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337 Fig. 6 – Comparison of Mrp antiporter MD simulations with protonation states set at different pH values. Panel A shows the RMSD of backbone atoms, panel B shows the number of water 338 molecules within 4 Å of all protein residues, and panel C shows the number of waters in the 339 340 functionally relevant central axis (Fig. 1), with the blue line showing the number of waters in 341 contact with protein observed in the cryo-EM structure. Data is shown as violin plots, where the shaded area is a KDE plot of all trajectory data and in the center is a box plot displaying 342 343 the median (white dot with the black box indicating the interquartile range). The total number 344 of positively and negatively charged residues at different pH are listed above panel A. 345

#### 346 Charge state assignment based on cryo-EM density

The above analysis highlights the importance of correct charge state description of protein, which is necessary for its stability during MD simulations. However, prediction of charge state by pKa calculations has its limitations. We thus attempted to deduce the protonation states 350 of amino acids from the high resolution cryo-EM data. Cryo-EM density maps can be used to 351 identify the charge states of acidic amino acid residues (glutamates and aspartates), because 352 neutral and negatively charged atoms have vastly different scattering amplitudes <sup>14, 17</sup> and 353 thus different cryo-EM density profiles. By carefully analyzing the cryo-EM density in our high-354 resolution maps, we obtained the charge states of selected glutamate and aspartate residues 355 and compared those to the pKa values obtained based on the modeled structure. We found 356 that there was an agreement between the charge state assignment based on the cryo-EM 357 maps (EMD-12742 for complex I and EMD-14124 for the Mrp antiporter) and the predicted 358 pKa based on the derived atomic models (PDBs 7071 and 7QRU, respectively). However, 359 several acidic residues showed discrepancies; the pKa calculations predicted some 360 carboxylates to be charge neutral that were assigned to be anionic by the cryo-EM density 361 analysis (Table 1). A possible explanation for this discrepancy is that although the protein 362 model-based pKa predictions are largely correct (especially for buried residues), the positions 363 of the (invisible) sidechains of charged glutamates and aspartates were incorrectly modeled, 364 resulting in overestimated structure-based pKas. To fix this discrepancy between the two 365 estimates, the cryo-EM density map of respiratory complex I (EMD-12742) was revisited. We remodeled the sidechains of selected residues that are predicted to be anionic based on 366 missing cryo-EM densities using Coot<sup>49</sup> and re-performed the pKa prediction on the new 367 368 model. A total of 7 glutamates and aspartates were remodeled one at a time (Table 1).

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Table 1 - Charge state of selected acidic amino acid residues in complex I from cryo-EM
 density data (EMD 12742) and pKa calculations, based on PDB 7071 coordinates or on a
 remodeled carboxylate sidechain. All carboxylates were remodeled independently.

<sup>a</sup> D67<sup>ND3</sup> was not remodeled, but instead the new pKa value is based on the structure with
 E147<sup>ND1</sup> remodeled.

	Density charge estimate	Original pKa	Remodeled pKa
E147 <sup>ND1</sup>	Charged	9.11	7.03
E206 <sup>ND1</sup>	Charged	8.85	6.37
E210 <sup>ND1</sup>	Charged	7.96	5.69
E231 <sup>ND1</sup>	Charged	7.44	6.56
D67 <sup>ND3</sup>	Neutral	7.18	9.34 <sup>a</sup>
E69 <sup>ND3</sup>	Charged	9.27	9.16
E30 <sup>ND4L</sup>	Charged	7.59	8.69
E66 <sup>ND4L</sup>	Charged	9.81	10.16

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The residues E231<sup>ND1</sup> and E147<sup>ND1</sup> of the functionally relevant E-channel in complex I <sup>43</sup> were 376 377 both predicted to be neutral based on pKa calculations but charged based on density analysis. 378 When pKa calculations were performed on re-modeled sidechains, it led to a drop in their 379 sidechain pKa and stabilization of their deprotonated states in good agreement with cryo-EM density-based assignment (Table 1). Interestingly, the remodeled sidechain conformation of 380 E147<sup>ND1</sup> not only improved the pKa of the residue itself, but also that of residues in its 381 382 surroundings, e.g. D67<sup>ND3</sup> (Fig. 7, Table 1). A similar improved agreement between pKa 383 prediction and cryo-EM-based charge state assignment was also observed for E206 and E210 384 from the ND1 subunit (Table 1), both of which are known to be central for protein function <sup>43</sup>. However, pKa predictions of E30 and E66 from ND4L, as well as E69 from ND3 could not be 385

improved despite their remodeled sidechains. One potential reason for this could be that the surroundings in two different conformations do not differ as drastically as in the other cases. Furthermore, the approximate nature of pKa predictions is well known, and with no explicit treatment of neighboring solvation can result in the overestimation of pKa values. All in all, remodeling of several sidechains not only improved the charged state assignment, but also improved the atomic modeling of cryo-EM density data (see discussion).

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Fig 7 - The remodeling of the sidechain of E147<sup>ND1</sup> (indicated by black arrow) improved its pKa as well as that of neighboring D67<sup>ND3</sup>. The first value of pKa is based on the original coordinates (PDB 7071), while the second value is after remodeling the sidechain of E147<sup>ND1</sup>.
 The cryo-EM density of the three residues is shown as grey mesh.

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## 399 Discussion

400 Protonation states of amino acids play a key role in protein structure stability and function. 401 However, it is extremely challenging to obtain an accurate estimate of the pKa of an amino 402 acid both by experiments and computations, and as a result in most cases, pKa values and 403 how they change during enzymatic action remains unknown. Because of this, MD simulations 404 are often performed by modeling amino acids in their fixed protonation states, including 405 standard charged states. Here we show that MD simulations of a membrane protein with all amino acids modeled in their standard charged states results in lower stability of the protein 406 407 overall and drives the conformation of the protein far from its starting point that is the cryo-408 EM conformation. Instead, if MD simulation is performed by fixing the charged states of 409 titratable amino acids based on pKa calculations, the conformational state remains closer to

the original structure. Our analysis of protein mobility and hydration, as well as residue-water
and residue-residue interactions supports this notion. Also, since the structural conformation
is retained in MD simulations performed after pKa calculations, we propose these more
closely match the charge states of amino acids that existed during the cryo-EM experiment.

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415 Our results also indicate that the relationship between protein stability and hydration is 416 strong, and that reduced hydration leads to a more stable simulation system which can 417 maintain important interactions. When leaving all protonatable residues in their standard 418 charged states, hydration is considerably enhanced, resulting in important protein-protein 419 interactions being broken, thereby reducing stability.

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421 The higher level of hydration observed in standard state simulations is primarily due to the 422 charged states of buried titratable amino acid residues. These charged amino acid residues in 423 the low protein dielectric interior create an unfavorable high-energy scenario due to poor 424 solvation. This establishes an electric field, pulling bulk water molecules into the protein and 425 enhancing solvation similar to the nanoscopic electroporation described earlier <sup>50</sup>, see also <sup>33</sup>. 426 We also note that protein hydration obtained from MD simulations performed in pre-defined 427 charge state is much closer to the structural hydration than that from the MD simulations 428 performed in standard state of the residues. Despite this, the hydration obtained from MD 429 simulations is in general higher than the hydration observed in the structure. The reason for 430 this discrepancy is in part due to the underestimation of protein hydration in the cryo-EM 431 maps, where only highly occupied and tightly bound water molecules can be observed.

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433 By performing MD simulations in pre-determined charge state from pKa calculations, one not 434 only investigates the state that was captured during structure resolution, but also its time 435 evolution more accurately. This is particularly useful in situations where there are a 436 particularly large number of titratable residues present in the protein with possible functional 437 relevance, such as in photosynthetic and respiratory enzymes, as well as proteins that couple 438 translocation of ions or metabolites to proton transfer reactions. However, empirical pKa 439 calculations or more thorough continuum electrostatics based pKa estimations have limited 440 accuracy and site-site interaction energy terms can often dominate, leading to large scale pKa 441 shifts with subtle changes in structure. Thus, it is important to use an accurate input model, 442 based on high-resolution data where there is less uncertainty in sidechain placements. Below ~2.5 Å resolution the correct rotamers of most sidechains can be confidently modeled, with 443 444 the key exception being negatively charged sidechains in cryo-EM maps, which have negative atomic scattering factors <sup>13, 17, 18</sup> and thus are usually invisible beyond the CB atoms. As 445 modeling and refinement programs do not take this into account, the sidechain orientation 446 447 of these residues is unreliable <sup>18</sup>. On the other hand, this fact makes it possible to deduce the 448 charge state of acidic residues from the cryo-EM density.

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Here we propose a method that may assist to improve modeling of sidechains of acidic residues. By performing fast empirical pKa calculations on the 3D model, pKas of all acidic residues can be estimated. If the predicted pKa value suggests a neutral state of an acidic residue that is expected to be anionic based on density analysis, this warrants remodeling of the sidechain of the amino acid. If the remodeled sidechain conformation yields a lower pKa, this is likely to be the more accurate conformation. By combining pKa calculations with sidechain remodeling on selected acidic residues of complex I, we show here that this is 457 feasible. In our future work, we aim to automate this process and obtain more accurate458 models of sidechains of acidic amino acid residues from the cryo-EM data.

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## 460 Methods

We performed all-atom molecular dynamics simulations of complex I from Yarrowia lipolytica 461 (PDB: 7071)<sup>43</sup> and Mrp antiporter from *Bacillus pseudofirmus* (PDB: 7QRU, altloc B)<sup>44</sup>. Both 462 proteins were placed in a mixed lipid bilayer and solvated with TIP3P and NaCl. Gromacs 463 versions 2020 and 2021 <sup>51</sup> were used for minimization, equilibration, and production runs. 464 465 Full details of the molecular dynamics set ups can be found in previous work on complex I<sup>43</sup> and Mrp antiporter<sup>44</sup>. The production runs were performed without any constraints in an NPT 466 ensemble, using Nosé–Hoover thermostat<sup>52, 53</sup> at 310 K and Parrinello-Rahman barostat<sup>54</sup> at 467 1 atm. We employed the LINCS algorithm to achieve a 2 fs timestep<sup>55</sup>, and the particle-mesh 468 Ewald method<sup>56</sup> with a cut-off of 12 Å to handle electrostatic interactions. The cut-off for van 469 470 der Waals interactions was 12 Å, with a switching distance of 10 Å. Table S5 lists the 471 simulations setups, and the S and P7 states for complex I and Mrp antiporter are extended 472 simulations from previous work. The P5, P6, P8, and P9 simulations of Mrp are new systems 473 constructed using the same protocol.

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Estimates of pKa were performed using the Propka software package<sup>39</sup>. The calculations were performed on the PDB structures of both complex I and Mrp. Asp, Glu and His were considered protonated (neutral) if their pKa was more than 7 in the P7 simulations, while Lys was considered deprotonated if its pKa was less than 7. The same process was performed in the P5, P6, P8, and P9 setups, with their respective pKa cutoffs changed. His was considered with the  $\delta$ -nitrogen protonated when neutral.

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482 Exponential fit of hydrogen bond decay was calculated using the SciPy *curve\_fit* function<sup>57</sup>. 483 We used a mono-exponential of the form  $y = me^{(-tx)} + b$ , where m, t, and b were 484 parameters that could vary. The quality of the fit was determined using R<sup>2</sup>, obtaining values 485 > 0.9. The half-life was calculated as  $t_{1/2} = t \times \ln 2$ .

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The electron density analysis and remodeling of the resolved structures was done using Coot<sup>49</sup>. The change in the glutamic and aspartic acid conformations was achieved with the rotamers function in Coot. The key requirement for the new position of the sidechain was a substantial deviation from its previous position, as well as avoiding clashes with its surroundings. Care was taken not to position the side chain in positive density.

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Visualization, analysis, and figure preparation was performed using VMD, Pymol and UCSF
 Chimera <sup>58</sup>.

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